

Lipid-Like Nanoparticles for Small Interfering RNA Delivery to Endothelial Cells

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Here, nanoparticles composed of lipid-like materials (lipidoids) to facilitate non-viral delivery of small interfering RNA (siRNA) to endothelial cells (ECs) are developed. Nanoparticles composed of siRNA and lipidoids with small size (~200 nm) and positive charge (~34 mV) are formed by self-assembly of lipidoids and siRNA. Ten lipidoids are synthesized and screened for their ability to facilitate the delivery of siRNA into ECs. Particles composed of leading lipidoids show significantly better delivery to ECs than a leading commercially available transfection reagent, Lipofectamine 2000. As a model of potential therapeutic application, nanoparticles composed of the top performing lipidoid, NA114, are studied for their ability to deliver siRNA targeting anti-angiogenic factor (SHP-1) to human ECs. Silencing of SHP-1 expression significantly enhances EC proliferation and decreases EC apoptosis under a simulated ischemic condition.

reported to facilitate non-viral delivery of siRNA, including direct conjugation of delivery reagent,^[7–10] formulation into liposomes,^[11,12] and encapsulation by polymers.^[13,14] Modification of siRNA with cholesterol,^[7] lipoprotein,^[8] peptide,^[9] or antibody^[10] has been reported to improve systematic siRNA delivery. Recently, systemic delivery of siRNA to the liver of non-human primates was demonstrated using a lipid formulation.^[11] Despite these advances in non-viral siRNA delivery, the diversity of published delivery materials still remains limited, in part due to their slow, multi-step syntheses.^[15] The customization of each synthetic reaction and multiple steps limits the ability to generate a significant library size with diversity.

1. Introduction

The specific silencing of gene expression through RNA interference (RNAi) has tremendous potential to address previously untreatable diseases.^[1–3] The safe and effective delivery of small interfering RNA (siRNA), however, remains challenging. Viral vector systems^[4,5] have demonstrated in vivo RNAi delivery efficacy but face several safety-related challenges, including potential immunogenicity.^[6] A variety of approaches have been

Recently, chemical approaches have been developed that allow the simple, rapid, and parallel generation of lipid-like delivery materials termed lipidoids as delivery agents for RNAi therapeutics.^[16] Lipidoid synthesis is based upon the conjugate addition of alkyl-acrylamides to primary or secondary amines. Synthesis can be performed in the absence of solvents, catalysts, or purification.^[16] A library of over 1 200 structurally diverse lipidoids has been synthesized, and members were shown efficacious in three species, including non-human primates.^[16–19]

During ischemic events, endothelial cells (ECs) can suffer from hypoxia-induced apoptosis. siRNA delivery to ECs may have utility in the treatment of ischemic disease by promoting angiogenesis or inhibiting apoptosis. To this end, we sought to develop a nanoparticulate, lipidoidal delivery system for the treatment of ECs under simulated ischemic conditions. Src homology 2 domain-containing protein tyrosine phosphatase-1 (SHP-1) has been known to inhibit EC proliferation and angiogenesis via the inactivation of vascular endothelial growth factor (VEGF) receptor-2 (KDR/Flk-1) in ECs.^[20–22] In addition to its anti-angiogenic activity, SHP-1 can directly affect apoptosis in many cell types^[23,24] by binding to death receptors such as TNFR-1 and FAS-R and blocking anti-apoptotic signals. Previous studies have demonstrated that SHP-1 expression is upregulated following myocardial or cerebral ischemia, which may contribute to the enhanced magnitude of myocardial^[25] or cerebral^[26] infarction. We hypothesized that siRNA-mediated silencing of SHP-1 expression could inhibit EC apoptosis and enhance EC proliferation, and thereby stimulate angiogenesis in ischemic tissue.

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2. Results and Discussion

2.1. Screening of Lipidoids for siRNA Delivery to Endothelial Cells

In vitro screening was performed to identify lipidoids that can deliver siRNA efficiently to ECs. Previously, 56 lipidoids were identified that were capable of delivering siRNA to HeLa cells with comparable knockdown efficiency to the commercially available in vitro transfection agent Lipofectamine 2000.^[16] Ten lipidoids were selected among those lipidoids and formulated at four different lipidoid/siRNA weight ratios (2.5 w/w, 5.0 w/w, 7.5 w/w, and 10.0 w/w), resulting in a total of 40 lipidoid/siRNA compositions. Lipidoids were synthesized through the conjugate addition of amine to acrylamide (Fig. 1A and B). Structural details of lipidoid (NA114) complexed without and with siRNA were visualized by negative-staining transmission electron microscopy (TEM), as shown in Figure 2A and B, respectively. These data showed that the lipidoid forms spherical particle with a size of 200 nm regardless of complexation with siRNA, which is consistent with the size distribution obtained from the dynamic light scattering (Fig. 2C). The tertiary amine of the lipidoids could be protonized in an acidic buffer (25 mM sodium acetate) used in this study, and hence result a positive charged particle. The lipidoids (NA114) loaded with and without siRNA have a zeta potential of 34 mV and 42 mV, respectively (Fig. 2C).

Lipidoid–siRNA formulations were tested for their ability to deliver siRNA targeting the housekeeping molecule (glyceraldehydes-3-phosphate dehydrogenase; GAPDH) to human umbilical vein endothelial cells (HUVECs). We identified 22 lipidoid formulations with delivery efficacy comparable to Lipofectamine

2000, two days after GAPDH siRNA transfection (Fig. 3A). The seven top-performing formulations with minimal cellular toxicity were further tested to deliver therapeutic siRNA to HUVECs. Two days after transfection of SHP-1 siRNA (siSHP-1) and green fluorescent protein siRNA (siGFP, as control siRNA; Fig. 3B), transfected HUVECs were transferred to hypoxic (1% oxygen) conditions with serum deprivation to simulate the low oxygen content and deficiency of survival growth factors in ischemic tissue.^[27] Two lipidoids, 110N₉-5 (“NA110”) and 114N₉-5 (“NA114”), were found to increase HUVEC viability significantly (NA110; $p < 0.05$ and NA114; $p < 0.01$), compared to respective controls (siGFP delivery, Fig. 3B). These data suggest these two lipidoidal formulations may provide vehicles for the treatment of ECs in ischemic tissues.

Previous studies have shown that top-performing lipidoids contain several structural similarities; i) amide linkages, ii) more than two alkyl tails, iii) tail length in the range of 8–12 carbons, and iv) one tail short of total substitution of the amine reactants, therefore containing one secondary amine.^[16] The lipidoids NA110 and NA114 identified as optimal for siRNA delivery to ECs showed structural similarities to 98N₁₂-5 (ND98), a lipidoid previously demonstrated to have activity in several in vivo models.^[16] NA110 is a branched version of ND98, while NA114 has one less ethyleneimine unit relative to ND98 (Fig. 1B and C).

2.2. Delivery of Therapeutic siRNA Using Lipidoids to Endothelial Cells

NA114, the optimal lipidoid identified in the present study, was used to deliver therapeutic siRNA (siSHP-1) into ECs and

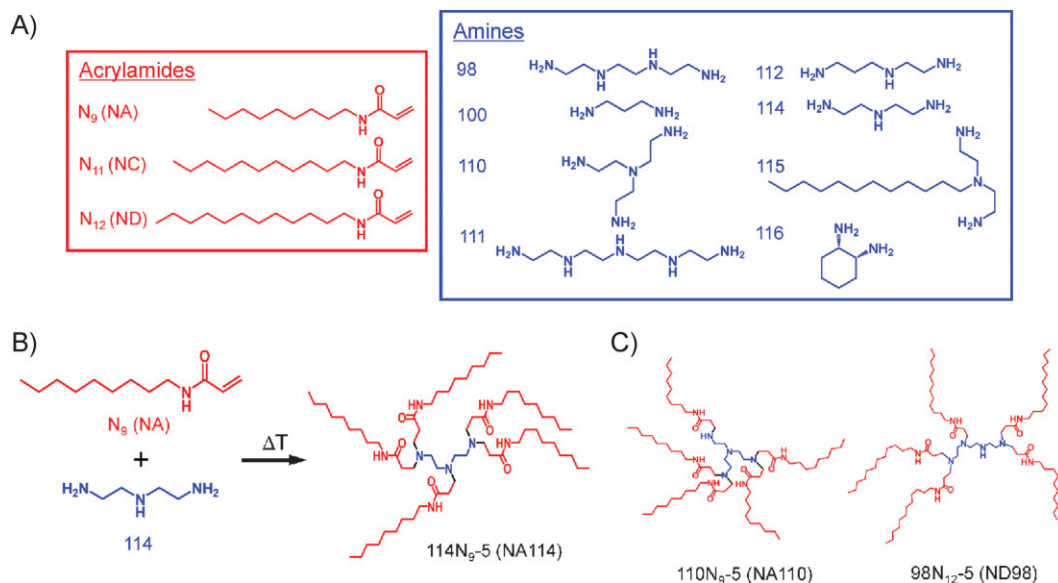


Figure 1. Synthesis of lipidoids for siRNA delivery. A) Alkyl-acrylamide and amine molecules were used to synthesize a combinatorial library of lipidoids. B) Lipidoid synthesis (114N₉-5; NA114) was performed through the conjugate addition of amine (114) to acrylamide (N₉; NA). Depending on the number of addition sites in the amino monomer, lipidoids can be formed with anywhere from 1 to 7 tails. Lipidoids are named as follows; (amine number) (acrylamide name) (the number of tails). For example, 100N₁₂-3 (ND100) indicates “the reaction of 100 with N₁₂ where 3 of 4 tails are present”. C) The molecular structures of 110N₉-5 (NA110) and 98N₁₂-5 (ND98).

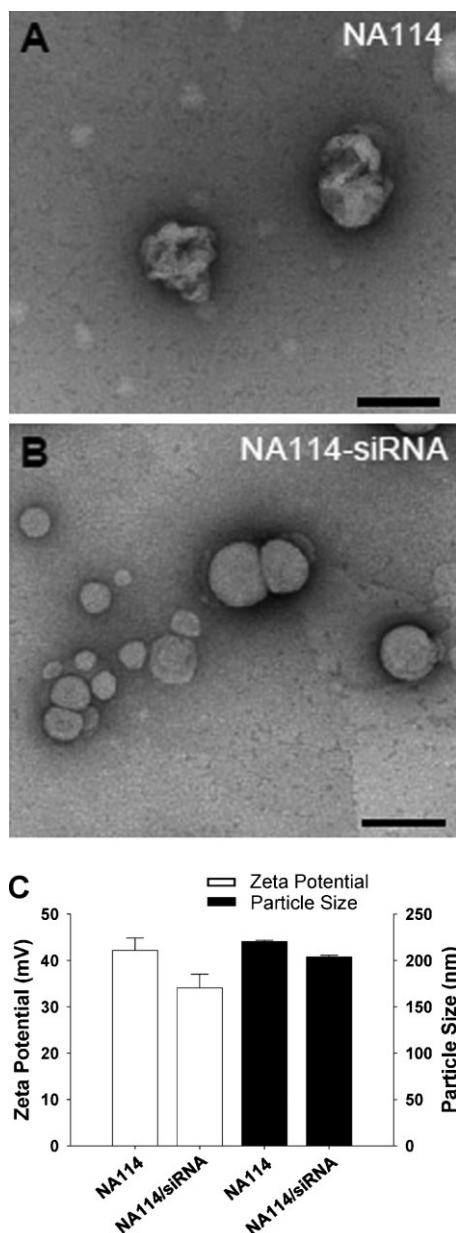


Figure 2. Characterization of lipidoid nanoparticles. TEM images of A) lipidoid (NA114) nanoparticles in the absence of siRNA and B) lipidoid (NA114) nanoparticles complexed with siRNA (5:1 weight ratio of lipidoid to siRNA). Scale bars indicate 200 nm. C) Zeta potential and particle size of lipidoid (NA114) and siRNA-lipidoid (NA114) nanoparticles (5:1 weight ratio of lipidoid to siRNA).

downregulate the target (SHP-1). Two days after siSHP-1 transfection with NA114, significant silencing of SHP-1 mRNA expression was achieved ($p < 0.05$) in siSHP-1-transfected HUVECs compared with siGFP-transfected HUVECs (Fig. 4A). In HUVEC culture using endothelial growth medium-2 (EGM-2) with 2% fetal bovine serum (FBS), SHP-1 knockdown using NA114-siRNA nanoparticles was similar to that by Lipofectamine 2000 (Fig. 4A). Importantly, under culture condition with higher serum content (10% FBS), NA114 showed significantly greater

SHP-1 silencing ($p < 0.01$) than Lipofectamine 2000 (Fig. 4B). Generally, the presence of serum can hinder intracellular delivery of nucleic acids.^[28] Thus, this lipidoid (NA114) may deliver more efficiently siRNA in the in vivo environment.

The silencing of SHP-1 by siRNA increased the expression of angiogenesis-inducing factors (e.g., KDR/Flk-1 and eNOS) in ECs (Fig. 5). Two days after siRNA delivery (transfection condition; EGM-2 with 2% FBS), siRNA-transfected HUVECs were moved to hypoxic (1% oxygen) condition with serum deprivation and cultured further for one and two days. While these conditions are known to increase SHP-1 expression,^[29] siSHP-1 transfection using NA114 resulted in significant knockdown of SHP-1 expression ($p < 0.01$), compared with siGFP transfection (Fig. 5A and B). The knockdown was maintained up to two days after culture (Fig. 5A and B), after which siRNA becomes diluted owing to cell division. Silencing of SHP-1 expression can induce activation of KDR/Flk-1, an important angiogenesis regulator in the VEGF signal pathway.^[20,21] The expression of eNOS could be enhanced via activation of KDR/Flk-1.^[20,21,29,30] siSHP-1 delivery mediated by NA114 increased KDR/Flk-1 expression and consequently eNOS expression in HUVECs (Fig. 5A, C, and D). The stimulation of KDR/Flk-1- and eNOS-mediated signal transduction may enhance angiogenesis in ischemic tissue and consequently reduce apoptosis of ischemic tissue.

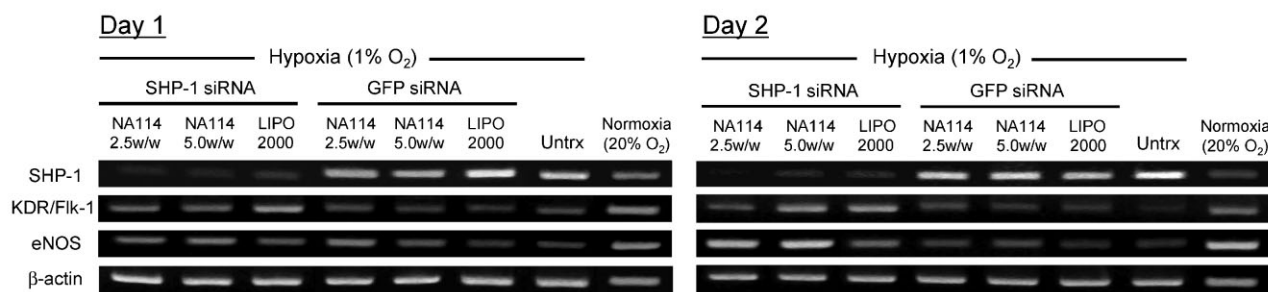
Intracellular delivery of siSHP-1 using NA114 inhibited apoptosis of ECs by hypoxia and serum deprivation. The favorable changes in gene expression profiles following siSHP-1 delivery (Fig. 5) substantially inhibited EC apoptosis and enhanced EC proliferation under hypoxic (1% oxygen) and serum-deprived condition (Fig. 6), which indicates that siSHP-1 therapy allows ECs to endure ischemic condition. On days one and two after culture under simulated ischemic condition, terminal deoxynucleotide transferase-mediated deoxyuridine triphosphate nick end-labeling (TUNEL) staining revealed that the portion of TUNEL-positive cells (apoptotic cells) in siSHP-1-transfected cell populations was significantly lower ($p < 0.01$) than that in siGFP-transfected cell populations (Fig. 6A and B). Additionally, siSHP-1-transfected HUVECs showed greater cell viability ($p < 0.01$) compared to siGFP-transfected HUVECs (Fig. 6C).

The capacity of ECs to generate microvessels was also enhanced by siSHP-1 delivery. When cultured on growth factor reduced (GFR)-Matrigel, siSHP-1-transfected HUVECs showed the formation of robust capillaries compared with siGFP-transfected HUVECs (Fig. 6A). The functional delivery of siSHP-1 to ECs may provide an avenue for the treatment of ischemic disease via the promotion of angiogenesis and/or inhibition of apoptosis. Of note, previous studies reported that injection of plasmid vector-based siRNA targeting SHP-1 enhanced angiogenesis and reduced the necrotic area in ischemic myocardium^[25] or hindlimb.^[31]

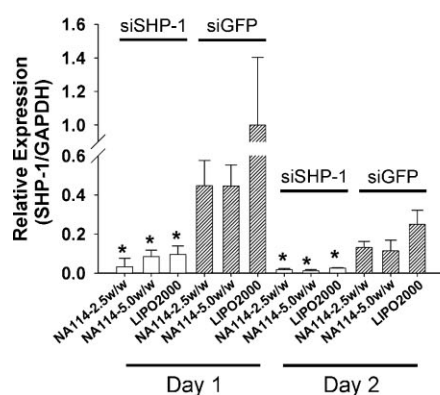
3. Conclusions

The study reported herein suggests that lipidoid-siRNA nanoparticles may provide a vehicle for the delivery of RNAi therapeutics to ECs. In particular, the formulations described here may provide a vehicle for the treatment of ischemic diseases such as myocardial, hindlimb, or cerebral ischemia. The

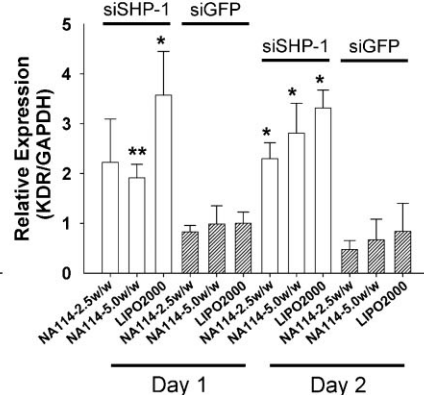
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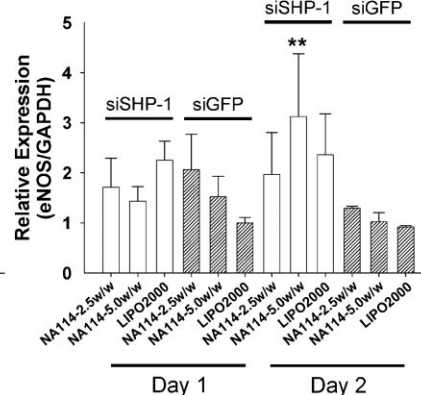
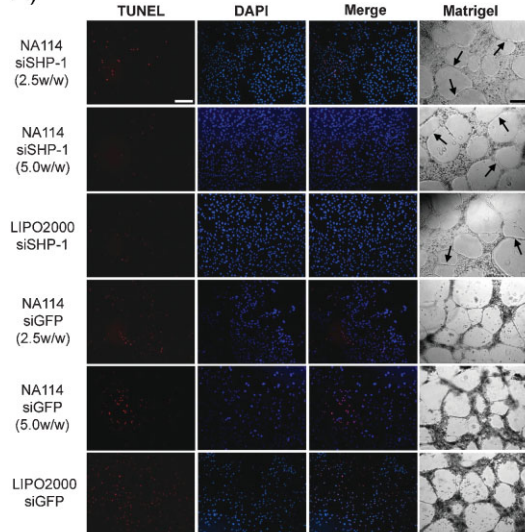
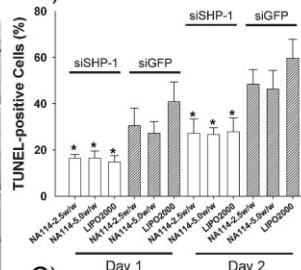


Figure 5. Gene expression profiles in siRNA-transfected HUVECs under hypoxic (1% oxygen) and serum-deprived (endothelial basal medium-2 (EBM-2) with no serum and growth factors) condition. A) RT-PCR for SHP-1, KDR/Flk-1, and eNOS of siRNA-transfected HUVECs at day 1 and 2 after culture. Quantitative real-time PCR for B) SHP-1, C) KDR/Flk-1, and D) eNOS. The gene expression in siRNA-transfected HUVECs ($n = 3$) at day 1 and 2 was normalized to that in siGFP-transfected HUVECs using Lipofectamine 2000 at day 1 (*: $p < 0.01$, **: $p < 0.05$, versus all siGFP groups at comparable time point).

A)



B)



C)

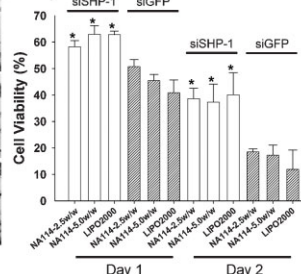


Figure 6. Inhibition of apoptotic activity in siSHP-1-transfected HUVECs cultured under hypoxic (1% oxygen) and serum-deprived (EBM-2 with no serum and growth factors) condition. A) TUNEL staining of siRNA-transfected HUVECs and capillary formation (arrows) by siRNA-transfected HUVECs at 2 days after culture ($\times 100$). Scale bars indicate 200 μm . B) The percentage ratio of TUNEL-positive cells (red; apoptotic cells) in DAPI-positive cells (blue; total cells) at day 1 and 2 after culture ($n = 4$, *: $p < 0.01$ versus all siGFP groups at comparable time point). C) The viability of siRNA-transfected HUVECs at day 1 and 2 after culture ($n = 4$, *: $p < 0.01$ versus all siGFP groups at comparable time point).

Transmission Electron Microscopy (TEM): Lipidoid/siRNA nanoparticles were formed as they were for transfection experiments (5:1 weight ratio of lipidoid to siRNA) and then droplets of the sample (5 μ L) were applied to hydrophilized carbon-covered copper grids (300 meshes) for 30 min. The sample was subsequently rinsed with contrasting material (1% uranyl acetate at pH 4.5). The remaining stain solution was removed with a filter paper and air-dried. TEM microstructure was determined using a Tecnai FEG TEM (FEI Tecnai 12 Spirit Bio-twin, FEI Company, Hillsboro, OR) operating at 80 kV.

GAPDH Activity Measurement: Transfection of GAPDH siRNA (siGAPDH) (Ambion, Austin, TX) was performed to screen optimal lipidoids for siRNA delivery to HUVECs. After 2 days of transfection, GAPDH activity in siRNA-transfected HUVECs was measured using KDalert GAPDH assay kit (Ambion). GAPDH activity of siGAPDH-transfected HUVECs was expressed as a percent activity to that of siGFP-transfected HUVECs. In this assay, reduction of GAPDH activity by cytotoxic or other non-specific effects is observed in both groups (siGAPDH group and siGFP group), while non-cytotoxic and specific silencing results in reduction of GAPDH activity only in siGAPDH group.

Cell Culture Under Hypoxic and Serum-Deprived Condition: Two days after transfection with siSHP-1 and siGFP, HUVECs were cultured under hypoxic and serum-deprived condition, a simulated ischemic condition. EGM-2 was changed to Endothelial Basal Medium-2 (EBM-2) without FBS and growth factors, and then siRNA-transfected HUVECs were further cultured for 1 or 2 days in a hypoxic incubator (MCO-18M, Sanyo, Japan) with air condition of 1% oxygen and 5% CO₂ at 37 °C. Low oxygen content was maintained through the controlled supply of nitrogen gas to the incubator.

Cell Viability Measurement: Cell viability was measured using the CellTiter 96 Aqueous One Solution assay kit (Promega, Madison, WI). Cellular metabolic activity was determined by measuring optical absorbance at 490 nm using a Victor3 Multilabel plate counter (Perkin-Elmer Life Sciences, Wellesley, MA). The viability of siRNA-transfected HUVECs cultured under hypoxic (1% oxygen) and serum-free (EBM-2) condition for 1 or 2 days was converted to percent viability by comparison to that of HUVECs cultured under normal condition with normoxia (20% oxygen) and complete growth medium (EGM-2) for the comparable time period.

Capillary Formation Assay: 48-well polystyrene plates were coated with Growth Factor Reduced (GFR)-Matrigel (BD Biosciences, San Jose, CA). Two days after transfection, siRNA-transfected HUVECs were detached with 0.05% (w/v) trypsin, suspended in EBM-2, and seeded at 4.0×10^4 cm² onto 48-well plates pre-coated with GFR-Matrigel. The cell plates were incubated under hypoxic (1% oxygen) condition at 37 °C and 5% CO₂. After culture of 2 days, the capillary structures generated by seeded HUVECs were examined microscopically.

Determination of Apoptotic Activity: On 1 and 2 days after culture under hypoxic and serum-free condition, apoptosis of siRNA-transfected HUVECs was investigated by the TUNEL method using a commercially available apoptosis detection kit (ApopTaq, Chemicon, Temecula, CA). Cells stained with rhodamine by TUNEL staining method were counter-stained with 4,6-diamidino-2-phenylindole (DAPI, Vector Laboratories, Burlingame, CA). The stained images were examined with a fluorescence microscope (Carl Zeiss, Oberkochen, Germany). The portion of TUNEL-positive cells in total cell populations was calculated as the percentage ratio of TUNEL-stained cells to DAPI-stained cells.

Reverse Transcription-Polymerase Chain Reaction (RT-PCR): Gene expression in HUVECs after siRNA transfection was examined with RT-PCR. Total RNA was isolated with RNeasy Mini kit (Qiagen, Chatsworth, CA) from each sample of the cells. A reverse transcription reaction was performed with 1 μ g of pure total RNA using SuperScript III reverse transcriptase (Invitrogen). The synthesized cDNA was amplified by PCR with human specific primers (SHP-1, KDR/Flk-1, eNOS, and β -actin) using Platinum PCR master mix (Invitrogen). The amplification conditions followed several steps; 5 min at 95 °C, followed by 25–35 cycles of denaturing (94 °C, 30 s), annealing (55–62 °C, 30 s), and extension (72 °C, 45 s) with a final extension at 72 °C for 7 min. The PCR products were visualized by electrophoresis on a 2% agarose gel with ethidium bromide (E-Gel, Invitrogen). β -actin was served as an internal control.

Quantitative Real-Time PCR (TaqMan Method): Quantitative real-time PCR was performed using a 7500 Fast Real-Time PCR System (Applied Biosystems, Foster City, CA). TaqMan Fast Universal PCR Master Mix (Applied Biosystems) was used for the reaction. Quantification of gene expression in HUVECs was analyzed with TaqMan Gene Expression Assays (Applied Biosystems) for each target (human SHP-1: Hs00169359_m1, human KDR/Flk-1: Hs00176676_m1, human eNOS: Hs00167166_m1, human GAPDH: Hs02758991_g1). The expression level of target genes was determined by the comparative C_t method, whereby the target was normalized to the endogenous reference (GAPDH).

Statistical Analysis: Quantitative data are expressed as mean \pm standard deviation. Statistical analysis was performed by the analysis of variance (ANOVA) using a Bonferroni test. A value of $p < 0.05$ was considered statistically significant.

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